

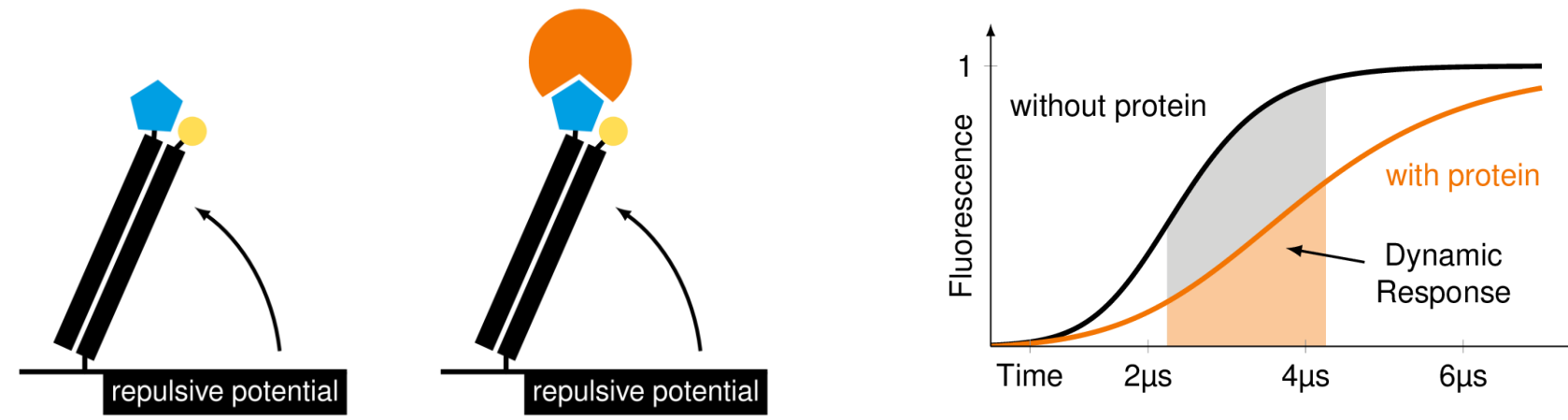
Advanced Biophysical Analysis of Mono- and Bispecific Antibody Formats with the switchSENSE® Biosensor Platform

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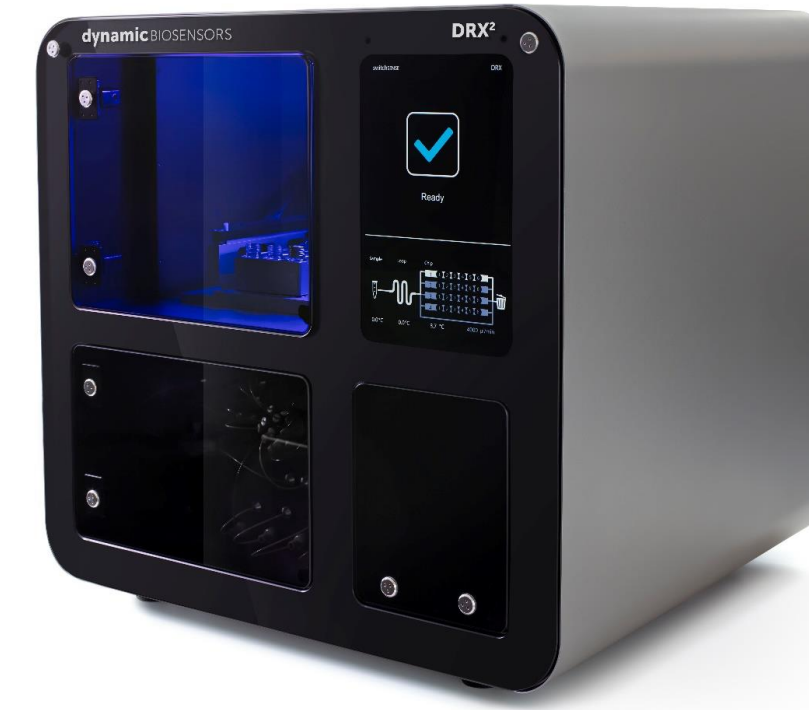
High-affinity and bispecific antibody formats are challenging analytes for interaction analysis systems. The apparent binding kinetics crucially depend on how the target molecules are presented on the sensor surface. In order to emulate the presentation of heterogeneous antigens on a cell surface with a biosensor platform, it is necessary to functionalize the sensor with different antigens at a defined stoichiometry. Further it is crucial to control the spatial arrangement of these antigens relative to each other, which has not been feasible up to now.

Here, we introduce the DNA-templated assembly of different ligands on a switchSENSE sensor and demonstrate the quantitative measurement of binding cooperativity, i.e., avidity effects. The influence of different ligand arrangements on the binding kinetics, in particular the off-rate, is discussed for antibody formats. We show how the ligand-to-ligand distance can be controlled with sub-nanometer precision using bifunctional DNA scaffolds, i.e. nanolevers with adjustable arm-lengths. We believe the introduced workflows will be highly instrumental in the discovery and selection of bispecific biotherapeutics.

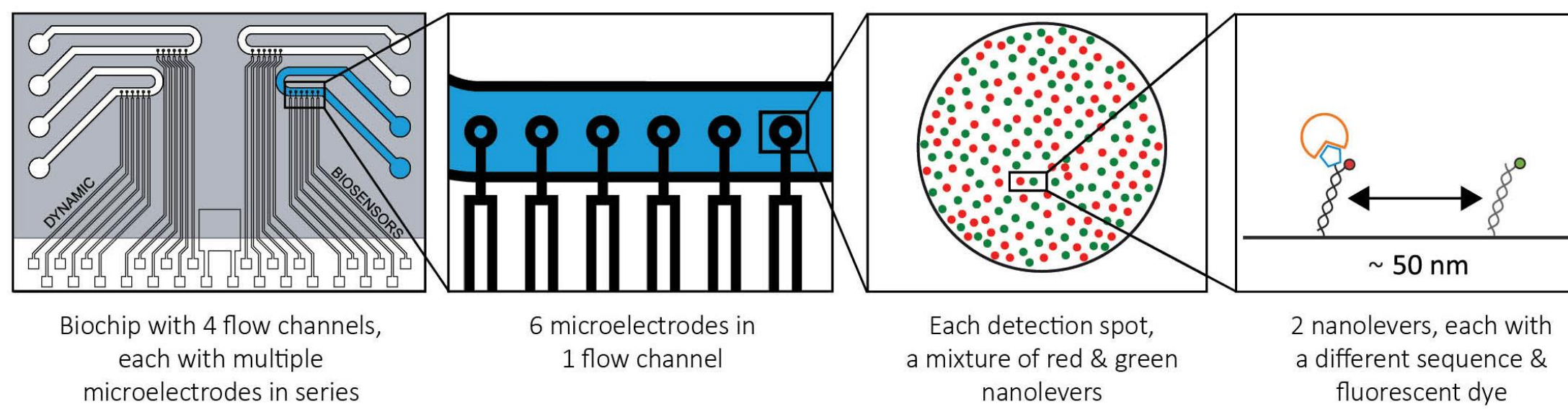
The switchSENSE® Principle | Electro-Switchable DNA Nanolevers



switchSENSE® DRX / DRX²



switchSENSE® Biochip



Interaction and Biophysical Analysis

- High Sensitivity**
Measurement of analyte concentrations from fM to mM
From ultra-fast to ultra-slow kinetics.
LOD = 10 fM
- Kinetics and Affinity**
Determination of binding rate constants k_{ON} , k_{OFF} and dissociation constants K_D in real-time.
- Size and Conformation**
Analysis of protein diameters on chip with 0.1 nm accuracy,
and monitoring of conformational changes.
- Cooperativity and Avidity**
Identification of multiple binding sites in a single measurement using variable capture molecule densities.
- Thermodynamics**
Characterization of melting transitions, thermal stability or thermodynamic analyses. 8° - 75°C

DNA nanolevers are electrically actuated at high-frequency on microelectrodes, while their orientation is monitored by time-resolved single photon counting. The binding of analyte molecules slows the switching dynamics in a characteristic way, providing an unprecedented level of information about the target.

Nature Commun. 4:2099 (2013) | Bioanal. Rev. 4 (2) 97-114 (2012) | JACS 134, 15225 (2012) | PNAS 107, 1397 (2010) | JACS 132, 7935 (2010)

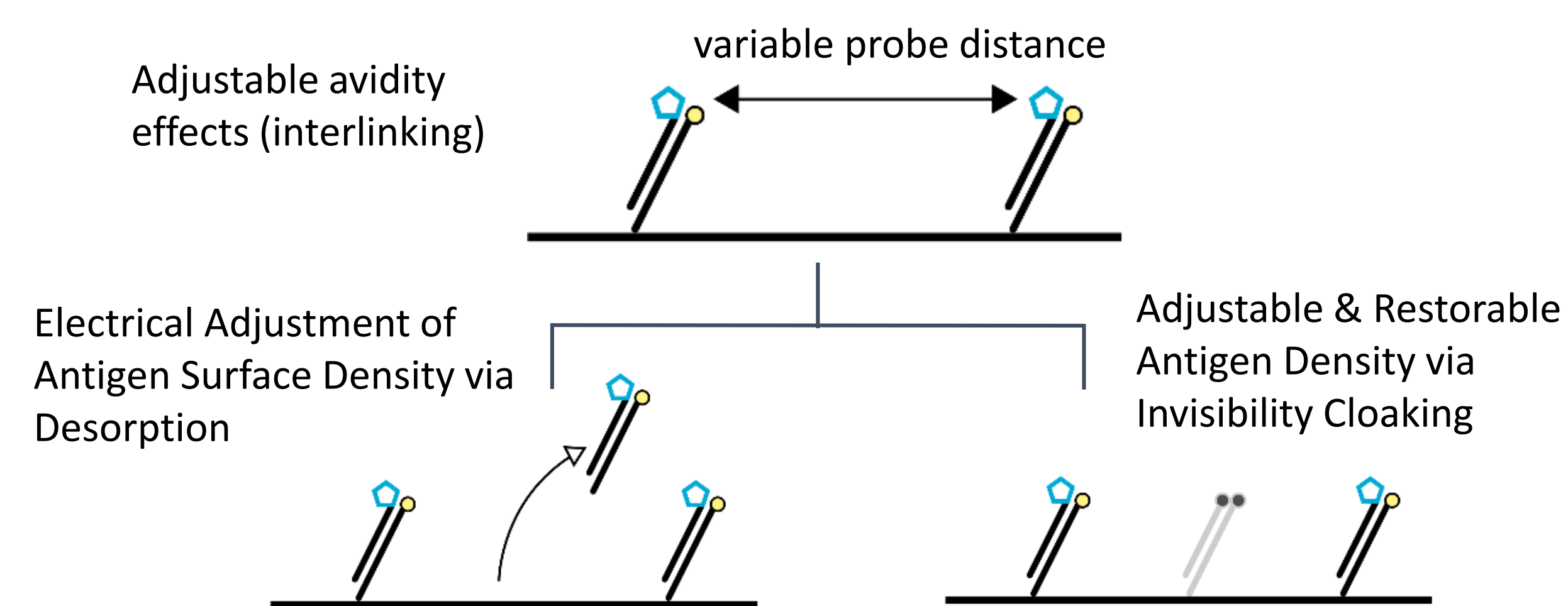
Control over Steric Configurations

Prerequisites for reliable kinetics measurements

| Phase | Potential meas. artifact | Cause | Consequence |
|--------------|---------------------------|--|---|
| Association | Mass-transport limitation | <ul style="list-style-type: none"> Ligand density too high Flow rate too low | → Apparent $k_{ON} < \text{real } k_{ON}$ |
| Dissociation | Rebinding | <ul style="list-style-type: none"> Ligand density too high Flow rate too low | → Apparent $k_{OFF} < \text{real } k_{OFF}$ |

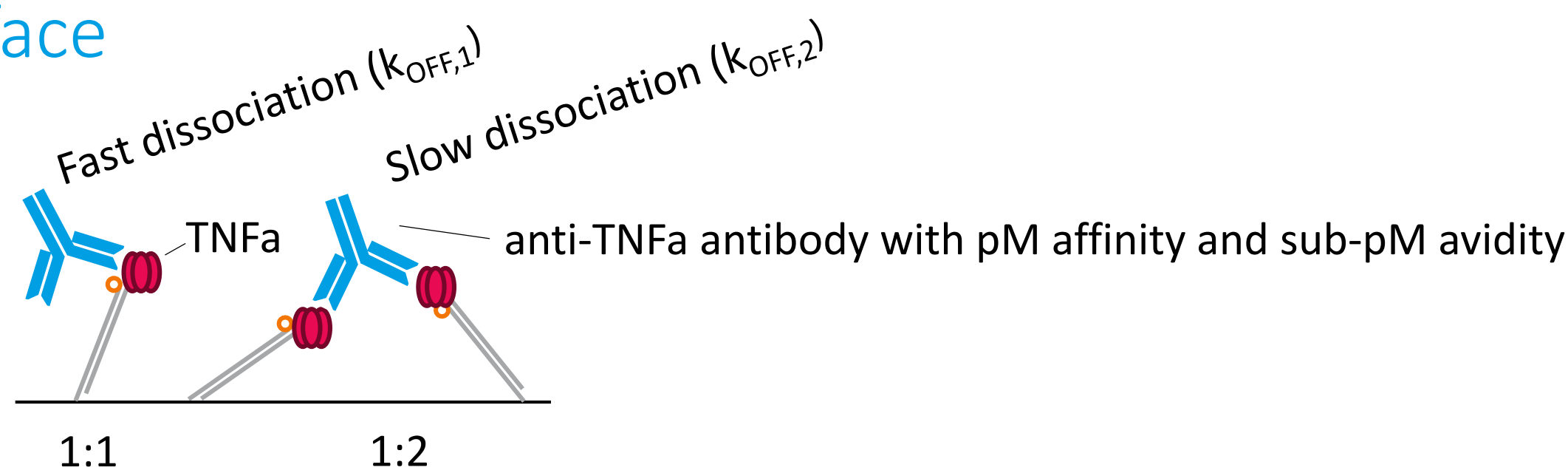
Adjust surface density of the ligand as low as possible & flow rate as high as possible

Biochip Surface Density Variation



switchSENSE provides the control over steric configurations of antigens and a homogenous surface density

Density Variation | IgG binding to an TNF α -modified surface



Complex binding situations → bi-phasic dissociation:

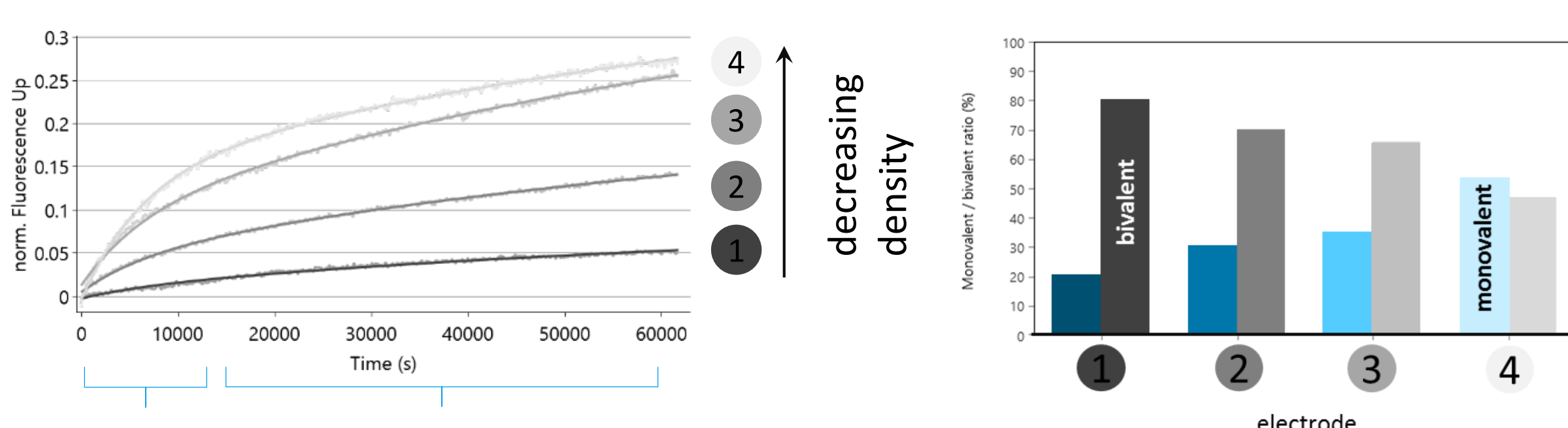
- Antibodies bound via one antigen binding site to ligand feature fast dissociation (fast $k_{OFF,1}$)
- Antibodies bound to two ligand feature slow dissociation rate (slow $k_{OFF,2}$)

→ By interlinking of both effects: slow and fast dissociation exists in parallel

Monovalent vs. Bivalent Binding – Affinity vs. Avidity

Adjusting the nanolever density → distinction between monovalent and bivalent binding (Affinity vs. Avidity)

Amplitudes reflect respective contributions of different dissociating species to the overall dissociation curve



monovalent phase $k_{OFF,1} = 1.55 \cdot 10^{-4} \text{ s}^{-1}$

bivalent phase $k_{OFF,2} = 0.12 \cdot 10^{-4} \text{ s}^{-1}$

Dissociation curves fitted with a global, double-exponential model:

Amplitudes of bi-phasic fit analysis reflect respective contributions

The thinner the ligand density the more dominant becomes the monovalent phase.

Bispecific Functionalization of Sensor Surface

Immobilization of Two Different Antigens with DRX² instrument

On-spot reference
Green and red fluorophore signal

More advanced assay

Detection of color-coded binding signals from individual antigens → analyzing bispecific binder

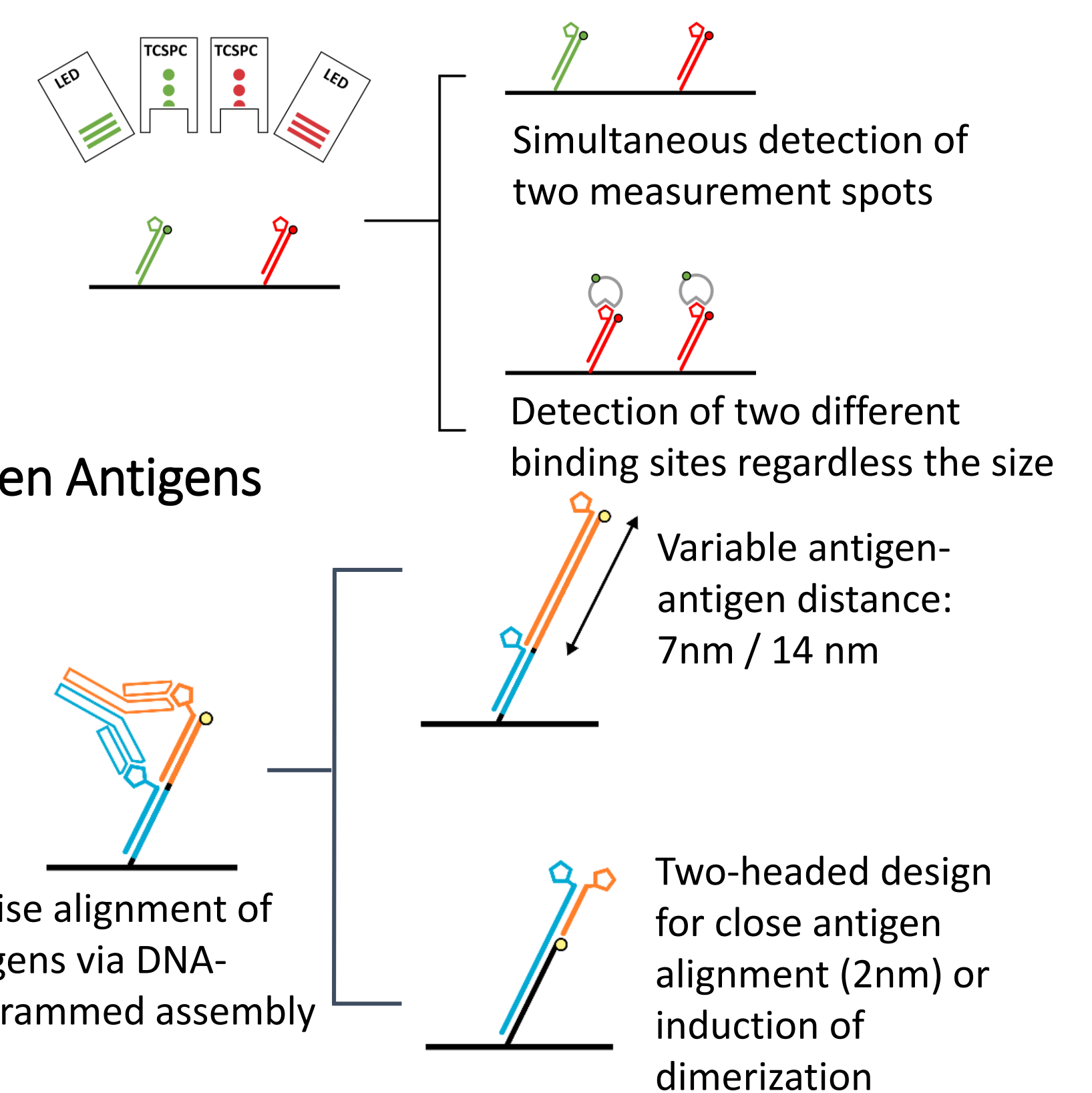
Bi-functional Nanolevers: Defined Distances between Antigens

Bispecific functionalization of the sensor surface

- Immobilization of **two antigens**
- Assembly of antigens at **defined distance** and **known position**
- Control over **surface density**

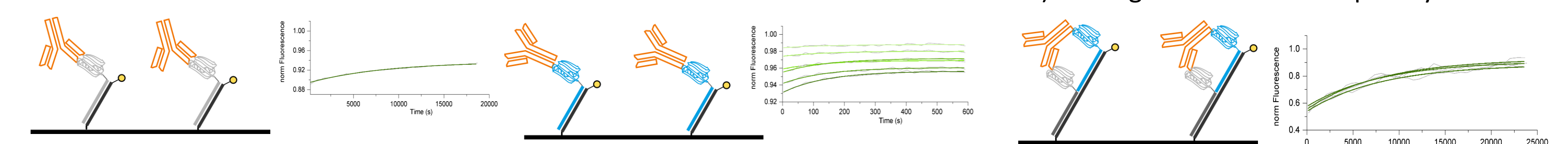
→ switchSENSE offers ultimate solution for understanding bivalent / bispecific antibody design & characterization of challenging bispecific antibody formats (femto-molar range)

Precise alignment of antigens via DNA-programmed assembly



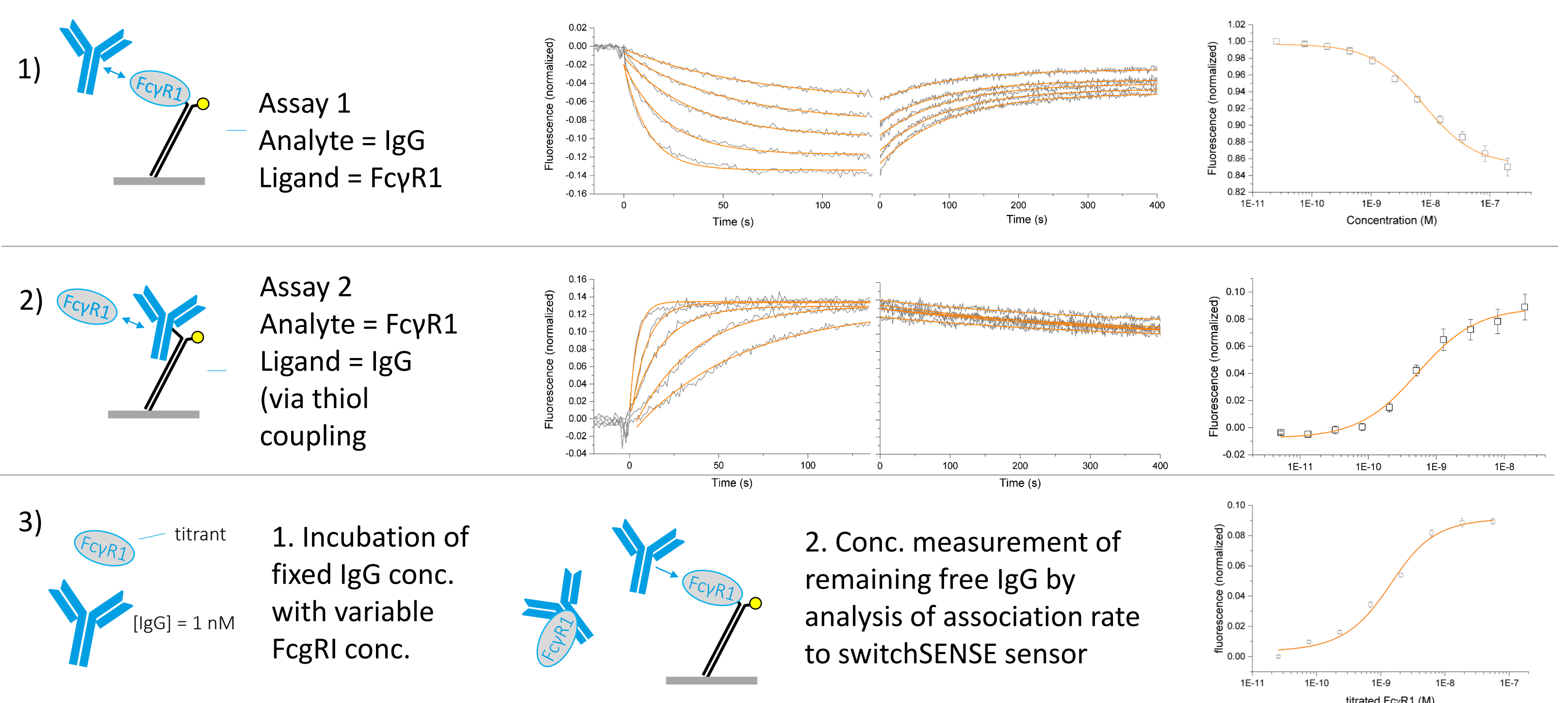
Bivalent Interaction | anti-TNF α – Fc γ R1

- 1) Homogeneous TNF α layer
- 2) Homogeneous Fc γ R1 layer
- 3) Homogeneous TNF α + Fc γ R1 layer



| Use of bifunctional nanolevers allows to study the contribution of a weak and strong binding site to the overall affinity. | Immobilized binding partner (Ligand) | k_{ON} ($10^6 \text{ M}^{-1} \text{ s}^{-1}$) | k_{OFF} (10^{-4} s^{-1}) | $K_D = k_{OFF}/k_{ON}$ |
|--|--|---|--|------------------------|
| | 1) TNF α layer | 23.7 ± 0.4 | 1.7 ± 0.1 | 6.9 ± 0.2 pM |
| | 2) Fc γ R1 | 1.4 ± 0.1 | 71 ± 4 | 4900 ± 400 pM |
| | 3) TNF α + Fc γ R1 layer | 20.0 ± 0.2 | 0.61 ± 0.09 | 3.0 ± 0.5 pM |

Assay Orientation & Solution Titration | Fc γ R1 – IgG binding



Fc γ R1 - IgG interaction supposed to follow 1:1 stoichiometry

| | Kinetics | | | Equilibrium Titration (Langmuir) |
|---|---|--|-----------------------------|----------------------------------|
| | k_{ON} ($10^6 \text{ M}^{-1} \text{ s}^{-1}$) | k_{OFF} (10^{-3} s^{-1}) | $K_D = k_{OFF}/k_{ON}$ (nM) | K_D (nM) |
| 1 | 1.21 ± 0.02 | 10.3 ± 0.1 | 8.50 ± 0.20 | 7.60 ± 1.00 |
| 2 | 3.69 ± 0.51 | 2.59 ± 0.17 | 0.70 ± .11 | 0.53 ± 0.09 |
| 3 | | n.a. | | 0.80 ± 0.17 |

- Affinity influenced by assay orientation and coupling strategy
- 10 fold weaker affinity of immobilized Fc γ R1 (overcome by in-solution competition assay)
- Complex formation of IgG and Fc γ R1 in solution: surface-bound ligands determine free fraction of IgGs yielding „true“ dissociation constant - a factor 10 lower than expected affinity of Fc γ R1 → matching K_D from kinetic measurements of immobilized IgG